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TRANSMITTAL LETTER TO THE UNITED STATES DESIGNATED/ELECTED OFFICE (DO/EO/US)

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Citation of References

Information Disclosure Statement by Applicant (Form PTO-1449)

ATTORNEY'S DOCKET NUMBER SANSYL002 U S APPLICATION NO. (If known, see 37 CFR 1.5)

CONCERNING A FILING UNDER 35 U.S.C. 371 INTERNATIONAL APPLICATION NO. PRIORITY DATE CLAIMED INTERNATIONAL FILING DATE PCT/EP00/06795 27 June 2000 28 June 1999 TITLE OF INVENTION: PHARMACEUTICAL DOSAGE FORMS FOR CONTROLLED RELEASE PRODUCING AT LEAST A TIMED PULSE APPLICANT(S) FOR DO/EO/US LEWIS, Gareth; MIGNONNEAU, Jérôme; and RIBARDIERE, Agnès ANDRE, Frédéric Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information: 1. This is a FIRST submission of items concerning a filing under 35 U.S.C. 371. This is a SECOND or SUBSEQUENT submission of items concerning a filing under 35 U.S.C. 371. 3. This express request to begin national examination procedures (35 U.S.C. 371(f)) at any time rather than delay examination until the expiration of the applicable time limit set in 35 U.S.C. 371(b) and PCT Articles 22 and 4. A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date. A copy of the International Application as filed (35 U.S.C. 371(c)(2)) a. \square is transmitted herewith (required only if not transmitted by the International Bureau). b. As been transmitted by the International Bureau. c. is not required, as the application was filed in the United States Receiving Office (RO/US). An English language translation of the International Application. Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371 (c)(3)) are transmitted herewith (required only if not transmitted by the International Bureau). have been transmitted by the International Bureau. have not been made; however, the time limit for making such amendments has NOT expired. A have not been made and will not be made. An English language translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371 (c)(3)). An executed oath or declaration of the inventor(s) (35 U.S.C. 371(c)(4)). 10. An English language translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371(c)(5)). Items 11. to 16. below concern document(s) or information included: An Information Disclosure Statement under 37 CFR 1.97 and 1.98. An assignment document for recording. A separate cover sheet in compliance with 37 CFR 3.28 and 3.31 is 12. included. 13. A FIRST preliminary amendment. A SECOND or SUBSEQUENT preliminary amendment. 14. A substitute specification. A change of power of attorney and/or address letter. 16. Other items or information:

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Patent Department				Paul E. Dupont	
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Attorney Docket No. SANSYL002

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Filing under 35 U.S.C. § 371 Corresponding to International Application No.: PCT/EP00/06795

Applicants: ANDRE, Frédéric; LEWIS, Gareth; MIGNONNEAU, Jérôme; and RIBARDIERE,

Agnès

International Filing Date: June 27, 2000

For: PHARMACEUTICAL DOSAGE FORMS FOR CONTROLLED RELEASE

PRODUCING AT LEAST A TIMED PULSE

CERTIFICATE UNDER 37 C.F.R. 1.10
Express Mail Label Number: EL676470337US
Date of Deposit: December 20, 2001
I hereby certify that this paper is being deposited with the United States Postal Service "Express Mail Post Office to Addressee" Service on the date indicated above and is addressed to: Commissioner for Patents, Box PCT, Atm: EO/US, Washington, DC 20231
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Commissioner for Patents Box PCT Attn: EO/US

Washington, DC 20231

Dear Sir:

PRELIMINARY AMENDMENT

Please amend the above-identified application as follows:

In the Claims:

Please amend claims 1-4, 6-9 and 11-22, cancel claims 5 and 10, and add new claims 23-34 as follows before calculating the filing fee for the above-identified application.

Please amend claims 1-4, 6-9 and 11-22 to read as follows:

- 1. (Amended) A delayed release coated core which produces a timed pulse release containing an active substance in its core and a polymer coating comprising one or more ammonio methacrylate copolymers, said core further containing one or more surfactants, one of said surfactants being capable of diffusing into the polymer coating and provoking a sudden change in the coating's properties.
- 2. (Amended) A delayed release coated core according to claim 1 wherein the surfactants are cationic or zwitterionic in nature.

- 3. (Amended) A delayed release coated core according to claim 2 wherein the ammonio methacrylate copolymers are of type A or B.
- 4. (Amended) A delayed release coated core according to Claim 3 wherein the cationic surfactants are chosen from trimethyl-dimyristoyl-ammonium propionate, dimethyl-dioctadecyl-ammonium bromide, trimethyl-cetyl-ammonium bromide, dimethyl-didodecyl-ammonium bromide, benzalkonium chloride, cetylpyridinium chloride and cetrimide and the zwitterionic surfactants are chosen from N-alylbetaines, C-alkylbetaines, N-alkylglycines, phosphatidylcholines and lecithins.
- 6. (Amended) A delayed release coated core according to claim 4 wherein the zwitterionic surfactant is cocamidopropylbetaine.
- 7. (Amended) A delayed release coated core according to Claim 3 wherein the active substance is chosen from diltazem, theophylline, felodipine, verapamil, clonidine, acebutolol, alprenolol, betaxolol, metoprolol, nadolol, propranolol, timolol, captopril, enalapril, fosinopril, tiapamil, gallopmil, amlodipine, nitrendipine, nisoldipine, nicardipine, felodipine, molsidamine, indomethacin, sulindac, indoprofen, ketoprofen, flurbiprofen, fenbufen, fluprofen, diclofenac, tiaprofenic acid, naproxen, mizolastin, terbulaline, salbutamol, betamethasone, prednisone, methylprednisone, dexamethasone, prednisolone, sumatriptan, naratriptan, cimetidine, ranitidine, famotidine, nizatidine, omeprozole, morphine, fenoprofen, ibuprofen, ketoprofen, alclofenac, mefenamic, alfuzosin, prazosin, tamulosin, levodopa and methyldopa, their salts and pharmacologically active esters.
- 8. (Amended) A delayed release coated core according to Claim 3 in the form of a particle, pellet, bead, granule or spheroid, of a diameter comprised between 0.3 and 3 mm.
- 9. (Amended) A delayed release coated core according to Claim 3 in the form of a tablet or a minitablet.
- 11. (Amended) A delayed release coated core according to Claim 3 wherein the core is separated from the polymer coating by a layer of water soluble polymer.

- 12. (Amended) A delayed release coated core according to claim 11 wherein the soluble polymer is chosen from hydroxypropylmethylcellulose, hydroxyethylcellulose and polyvinylpyrrolidone.
- 13. (Amended) A pharmaceutical dosage form compromising a delayed release coated core according to Claim 3.
- 14. (Amended) A pharmaceutical dosage form according to claim 13 in the form of a tablet, a multilayer tablet, a multicoated tablet or a capsule.
- 15. (Amended) A pharmaceutical dosage form according to claim 13 wherein coated cores of differing delayed release times are combined together to give a "stepped" release profile.
- 16. (Amended) A pharmaceutical dosage form according to claim 13 wherein the delayed release coated core is combined with another galenic entity, the release of said entity being immediate or sustained.
- 17. (Amended) A pharmaceutical dosage form according to claim 16 wherein the other galenic entity contains an active substance different from the active substance in the delayed release coated core.
- 18. (Amended) A pharmaceutical dosage form according to claim 16 wherein a first release pulse occurs immediately and a second release pulse is delayed for a fixed time.
- 19. (Amended) A capsule according to claim 16 comprising a delayed release coated core in the form of a particle, pellet, bead granule or spheroid having a diameter of 0.3 to 3 mm or in the form of a minitablet, and an immediate and/or sustained release entity chosen from
- (i) immediate release particles or minitablets or an immediate release granulate or powder, and
 - (ii) controlled release particles or minitablets.
- 20. (Amended) A tablet according to claim 16 wherein the delayed release coated core in the form of a particle, pellet, bead granule or spheroid having a diameter of 0.3 to 3 mm is imbedded in a rapidly disintegrating matrix.

- 21. (Amended) A capsule according to claim 16 comprising one or more immediate release tablets and one or more delayed release coated cores in the form of tablets.
- 22. (Amended) A multicoated tablet according to claim 16 coated with an immediate release soluble or disintegrable coating.

Please cancel claims 5 and 10

Please add the following new claims:

- --23. (New) A tablet according to claim 20 wherein the matrix is free of active substance.
- 24. (New) A tablet according to claim 20 wherein the matrix also contains active substance.
- 25. (New) A tablet according to claim 20 wherein sustained release particles are mixed with the delayed release coated particles.
- 26 (New) A tablet according to claim 20 wherein immediate release particles are mixed with the delayed release coated particles.
- 27. (New) A tablet according to claim 20 wherein the delayed release coated particles are further coated with a layer containing the active substance.
- 28. (New) A tablet according to claim 20 comprising one or more layers containing the delayed release particles in the rapidly disintegrating matrix and one or more layers containing the active substance in an immediate release matrix.
- 29. (New) A delayed release coated core according to claim 3, said core further containing a pharmaceutically acceptable organic acid.
- 30. (New)) A delayed release coated core according to claim 4, said core further containing an acid chosen from maleic, tartaric, malic, fumaric, lactic, citric, adipic and succinic acid or a salt thereof.
- 31. (New) A delayed release coated core according to claim 30 wherein the acid is chosen from tartaric, fumaric, citric and succinic acid or salt thereof.
- 32. (New) A delayed release coated core according to claim 31 wherein the acid is succinic or tartaric acid and the surfactant is cetylpyridinium chloride or cocamidopropylbetaine.
- 33. (New) A delayed release coated core according to claim 32 wherein the active substance is alfuzosin or an acid-addition salt thereof.
- 34. (New) A delayed release coated core according to claim 32 wherein the active substance is a hypnotic.--.

REMARKS

Claims 1-4 and 6-22 have been amended in order to write these claims in the appropriate U.S. claim format, correct errors of spelling and syntax, and eliminate multiple dependencies. Amended claim 4 combines original claims 4 and 5, and amended claim 9 combines original claims 9 and 10.

Claims 5 and 10 have been canceled.

Claims 23-34 have been added by the foregoing amendments. Claims 23-28 are directed to alternative elements (i)-(iv) of original claim 20.

Claims 29-32 are directed to delayed release coated cores containing an organic acid. Support for these claims is found in the specification, for example, at page 5, line 31 to page 6, line 5 and Examples 1-3.

Claims 32-34 further specify the organic acid, the surfactant and the active substance. Support for these claims is found in the specification, for example, at page 6, lines 4-5, page 4, line 29 to page 5, line 6, page 5, lines 11-29 and Examples 1-3.

Claims 1-4, 6-9 and 11-34 are in the application as amended.

Attached hereto is a marked-up version of the changes made to the claims by the instant amendment. The marked-up version is entitled "Version With Markings To Show Changes Made".

Date: 14 20/6/

Paul E. Düpont Reg. No. 27,438

Respectfully submitted,

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10/019588 53! Record 20 DEC 2001 Version With Markings to Show Changes Made

In the Claims:

Claims 1-4 and 6-22 have been amended as follows:

- 1. (Amended) A delayed release coated core [producing] which produces a timed pulse release [comprising] containing an active substance in its core and a polymer coating comprising [at least] one or more ammonio methacrylate copolymers, [characterised in that the] said core [comprises at least] further containing one [ore] or more surfactants, one of said surfactants being [a means that diffuses] capable of diffusing into the polymer coating and [at a given level provokes] provoking a sudden change in the coating's properties.
- 2. (Amended) A delayed release coated core according to claim 1 [, characterised in that] wherein the surfactants are cationic or zwitterionic in nature.
- 3. (Amended) A delayed release coated core according to claim 2 [1 or 2, characterised in that] wherein the ammonio methacrylate copolymers are of type A or B.
- 4. (Amended) A delayed release coated core according to [anyone of claim 1 to 3, characterised in that] Claim 3 wherein the cationic surfactants are chosen [among] from trimethyl-dimyristoyl-ammonium propionate, dimethyl-dioctadecyl-ammonium bromide, trimethyl-cetyl-ammonium bromide, dimethyl-didodecyl--ammonium bromide, benzalkonium chloride, cetylpyridinium chloride and cetrimide and the zwitterionic surfactants are chosen from N-alylbetaines, C-alkylbetaines, N-alkylamidobetaines, N-alkylglycines, phosphatidylcholines and lecithins.
- 6. (Amended) A delayed release coated core according to claim 4 wherein [5, characterised in that] the zwitterionic surfactant is [cocamidopropylbetain] cocamidopropylbetaine.

- 7. (Amended) A delayed release coated core according to [anyone of claim 1 to 6, characterised in that] Claim 3 wherein the active substance is chosen [among] from diltazem, theophylline, felodipine, verapamil, clonidine, acebutolol, alprenolol, betaxolol, metoprolol, nadolol, propranolol, timolol, captopril, enalapril, fosinopril, tiapamil, gallopmil, amlodipine, nitrendipine, nisoldipine, nicardipine, felodipine, molsidamine, indomethacin, sulindac, indoprofen, ketoprofen, flurbiprofen, fenbufen, fluprofen, diclofenac, tiaprofenic acid, naproxen, mizolastin, terbulaline, salbutamol, betamethasone, prednisone, methylprednisone, dexamethasone, prednisolone, sumatriptan, naratriptan, cimetidine, ranitidine, famotidine, nizatidine, omeprozole, morphine, fenoprofen, ibuprofen, ketoprofen, alclofenac, mefenamic, alfuzosin, prazosin, tamulosin, levodopa and methyldopa, their salts and pharmacologically active esters.
- 8. (Amended) A delayed release coated core according to [anyone of claim 1 to 7, characterised in that it is] Claim 3 in the form of a particle, pellet, bead, granule or spheroid, of a diameter comprised between 0.3 and 3 mm.
- 9. (Amended) A delayed release coated core according to [anyone of claim 1 to 7, characterised in that it is Claim 3 in the form of a tablet or a minitablet.
- 11. (Amended) A delayed release coated core according to [anyone of claim 1 to 10, characterised in that] Claim 3 wherein the core is separated from the polymer coating by a layer of water soluble polymer.
- 12. (Amended) A delayed release coated core according to claim 11 [, characterised in that] wherein the soluble polymer is chosen [among] from hydroxypropylmethylcellulose, hydroxyethylcellulose and [polyvinylpyrolidone] polyvinylpyrrolidone.
- 13. (Amended) A pharmaceutical dosage form compromising [at least] a delayed release coated core according to [anyone of claims 1 to 12] Claim 3.

- 14. (Amended) A pharmaceutical dosage form according to claim 13 [, characterised in that it takes] in the form of a tablet, a multilayer tablet, a multicoated tablet or a capsule.
- 15. (Amended) A pharmaceutical dosage form according to claim 13 [or 14, characterised in that] wherein coated cores of differing delayed release times are combined together to give a "stepped" release profile.
- 16. (Amended) A pharmaceutical dosage form according to claim 13 [or 14, characterised in that] wherein the delayed release coated [core(s) is/are] core is combined with [other] another galenic [entitie(s), which] entity, the release [is] of said entity being immediate or sustained.
- 17. (Amended) A pharmaceutical dosage form according to claim 16, characterised in that] wherein the other galenic [entitie(s) contain(s) a different] entity contains an active substance [as] different from the active substance in the delayed release coated [core(s)] core.
- 18. (Amended) A pharmaceutical dosage form according to claim 16 [, characterised in that] wherein a first release pulse occurs immediately and a second release pulse is delayed to for a fixed time.
- 19. (Amended) A capsule according to claim 16 [, characterised in that it comprises the] comprising a delayed release coated [cores according to claim 8 or 10] core in the form of a particle, pellet, bead granule or spheroid having a diameter of 0.3 to 3 mm or in the form of a minitablet, and an immediate and/or sustained release entity chosen [alternatively among] from
- (i) immediate release particles or minitablets or an immediate release granulate or powder, and
 - (ii) controlled release particles or minitablets.

20. (Amended) A tablet according to claim 16 [, characterised in that it comprises] wherein the delayed release coated core in the form of a particle, pellet, bead granule or spheroid having a diameter of 0.3 to 3 mm is [cores according to claim 8] imbedded in a rapidly disintegrating matrix [and alternatively in that

- (i) the matrix is free of the active substance,
- (ii) the matrix also comprises the active substance,
- (iii) sustained release particles are mixed to the delayed release particles,'
- (iv) immediate release particles are mixed with the delayed release coated particles,
- (v) the delayed release particles are further coated with a layer comprising the active substance, allowing an immediate release,
- (vi) the tablet consists of one or more layers comprising the delayed release particles in the rapidly disintegrating matrix and of one or more layers comprising the active substance in an immediate release matrix.
- 21. (Amended) [Capsule] A capsule according to claim 16 [, characterised in that it comprises] comprising one or more immediate release tablets and one or more delayed release [tablets according to claim 9] coated cores in the form of tablets.
- 22. (Amended) A multicoated tablet [Multicolored tablets] according to claim 16 [, characterised in that the tablet is] coated with an immediate release soluble or disintegrable coating.

Claims 5 and 10 have been canceled.

Claims 23-34 have been added.

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PHARMACEUTICAL DOSAGE FORMS FOR CONTROLLED RELEASE PRODUCING AT LEAST A TIMED PULSE

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The present invention relates to controlled release dosage forms producing at least a timed pulse, that is a rapid and complete controlled release of a pharmaceutical substance a fixed time after administration.

Most pharmaceutically active substances administrated orally are given as conventional immediate release or rapid release forms. Thus, provided drug release and absorption are rapid, the concentration time profile of the active substance in the blood or other body compartment depends on the kinetics of elimination of the molecule from the body, and on the distribution and kinetics of distribution in different body compartments and tissues.

This limits the time the drug spends in the body components and thus the time of action of the drug. For this reason, in order to increase the residence time of the drug, prolonged release dosage forms are used, allowing less frequent dosing. In the past, it has often been considered for most drugs that there is an optimum plasma level, and thus the best formulation will be one that gives blood plasma concentration profiles as near constant as possible, and allows reduced dosing frequency.

However such release patterns giving constant plasma levels are not always optimal.

Physiological processes are indeed most of the time not constant over time and circadian rhythms have been shown for almost all bodily functions, as well as symptoms of certain diseases.

For example, myocardial infarction and ischemia and angina pectoris, attacks are more frequent in morning hours 6 - 12 am, and occur particularly in the 4 hours following awaking. Thus it would be preferable in the treatment of these diseases to ensure relatively high blood levels of the drug over that period. For example, an evening administration at 21.00 could then imply an increased release rate about 7-10 hours after administration.

Examples of other diseases and symptoms showing a circadian pattern are inflammatory diseases, nocturnal asthma, migraine headache, ulcer, including perforated ulcer, intractable pain and pain from rheumatoid arthritis.

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Controlled release dosage forms producing a timed pulse are therefore particularly adapted in the treatment of the here above cited diseases and symptoms thereof. In other words, they can be used for the corresponding chronotherapeutic treatments.

It is also well known that drug release in the form of a pulse rather than a steady slow release may reduce loss by a saturable first-pass effect as in the case of levadopa or propoxyphene. In addition, certain receptors are inactivated by prolonged stimuli, and a pulsed, or on-off delivery can overcome this effect.

As another advantage timed release can allow targeting of a drug to a given site of the gastrointestinal tract, in particular the colon. This depends on the near constant transit time of a pharmaceutical dosage form through the small intestine. A rapid release of the drug in the colon may have advantages in allowing a high local concentration and improved absorption, since absorption of many drugs is much slower and less complete from the colon than from the small intestine, and absorption may become the rate-limiting step rather than release from the dosage form.

It is therefore clear that formulations producing a timed pulse are useful, for example, as described above, for obtaining a non-constant blood plasma concentration profile compatible with and optimal for the therapeutic objective, or for compensating the differences in the rate and extent of absorption in different portions of the gastro-intestinal tract, and so obtaining minimally fluctuating blood levels over the entire dosing period.

Dosage forms for controlled release producing at least a timed pulse may also be useful as complementary treatment of an initial treatment. For example, the effect of an initial active substance, which acts rapidly may be suppressed or completed by a second active substance released a fixed time after administration of the dosage form comprising both of the active substances.

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Until now, one of the known methods of achieving a timed pulse from a single galenic entity consists in coating a core comprising the active substance with a polymer coating comprising at least one or more methacrylate copolymers containing quaternary ammonium groups. These are referred to as ammonio methacrylate copolymers.

Dosage forms formulated from these here above described coated cores can give sigmoidal release profiles but not real timed pulse profiles. In other words the achieved release rate is often not rapid enough. And another disadvantage of this technique is related to the fact that a large amount of the drug is not released from the coated cores.

The first object of the present invention is then related to a pharmaceutical dosage form for a timed pulse release, whereby the release rate is zero or very low during a fixed time and then the whole of the drug comprised in the dosage form is released rapidly.

Indeed the applicant has found surprisingly that the addition of small quantities of a surfactant into a core comprising the active substance, which is coated with at least one or more ammonio methacrylate copolymer, as described above, give a delayed accelerated pulse, and substantially more complete release of the drug.

The term "particle" in the whole description encompasses all galenic entities variously known as pellets, beads, granules or spheroids.

The core may be a tablet or a particle and the dosage form may be monolithic, that is a single tablet, or multiparticulate, that is either several tablets or a large number of particles. Multiple particles may be within a capsule. Alternatively a large number of particles may be compressed into a tablet which disintegrates in aqueous fluids, releasing the particles.

For reasons of simplicity, in the whole description, the resulting particle or tablet is named "delayed release particle", or "delayed release tablet" or more generally "delayed release coated core".

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Thus the present invention, as a first object, provides delayed release coated cores comprising an active substance in their core and a polymer coating comprising at least one or more ammonio methacrylate copolymer, characterised in that the core comprises at least a surfactant.

The present invention also provides monolithic or multiparticulate pharmaceutical dosage forms comprising such delayed release coated cores, producing one unique timed pulse.

The present invention also provides the method of manufacture of the delayed release coated cores and the pharmaceutical dosage forms containing them.

Ammonio methacrylate can be of two types, A and B. These are for example marketed by Röhm Pharma as Eudragit[®] RS and Eudragit[®] RL, respectively. Type A, like Eudragit[®] RS, is relatively impermeable to water and small molecules, and Eudragit[®] RL is relatively permeable.

According to the invention other polymers and pharmaceutical adjuvants well known to persons with ordinary skill in the art of pharmaceutical formulation may also be incorporated in the coating. The polymers may include cellulosic derivatives such as ethylcellulose or hydroxypropylmethylcellulose (ou hypromellose), and other adjuvants are plastifiers such as diacetylated monoglycerides or triethyl citrate, and antitack agents such as talc.

According to the present invention the additional surfactant is either cationic or amphoteric and/or zwitterionic in nature.

In fact, an additional surfactant diffuses into the polymer coating, and at a given level provokes a sudden change in the film's properties.

Examples of such cationic surfactants are trimethyl-dimyristoyl-ammonium propionate, dimethyl-dioctadecyl-ammonium bromide, trimethyl-cetyl-ammonium bromide (CTAB), dimethyl-didodecyl-ammonium bromide (DDAB(12)), benzalkonium chloride, cetylpyridinium chloride or cetrimide.

Other salts of the above cationic surfactants may equally be employed.

Preferred examples of cationic surfactants are benzalkonium chloride and cetylpyridinium chloride.

Examples of zwitterionic surfactants are the N-alkylbetaines, the C-alkylbetaines, the N-alkylamidobetaines such as cocamidopropylbetain; the N-alkylglycines and the phosphatidylcholines or lecithins.

The present invention also extends to the use of mixtures of cationic and/or zwitterionic surfactants especially mixtures of the afore mentioned surfactants.

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Suitable active substances may be selected from, for example, hormones, polysaccharides, polypeptides, steroids, hypnotics and sedatives, psychic energizers, tranquilizers, anticonvulsants, muscle relaxants, antiparkinson agents, analgesics, anti-inflammatories, muscle contractants, sympathomimetics, polypeptides and proteins capable of eliciting physiological effects, diuretics, lipid regulating agents, antiandrogenic agents, neoplastics, antineoplastics, hypoglycemics, antienteritis agents, and diagnostic agents.

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Exemples of active substance useful in this invention include diltiazem, theophylline, felodipine, verapamil, clonidine, acebutolol, alprenolol, betaxolol, metoprolol, nadolol, propranolol, timolol, captopril, enalapril, fosinopril, tiapamil, felodipine, nicardipine, nitrendipine, nisoldipine, amlodipine, gallopamil. molsidamine, indomethacin, sulindac, indoprofen, ketoprofen, flurbiprofen, fenbufen, fluprofen, diclofenac, tiaprofenic acid, naproxen, mizolastin, terbutaline, salbutamol, betamethasone, prednisone, methylprednisone, dexamethasone, prednisolone, sumatriptan, naratriptan, cimetidine, ranitidine, famotidine, nizatidine, omeprozole, morphine, fenoprofen, ibuprofen, ketoprofen, alclofenac, mefenamic, alfuzosin, prazosin, tamsulosin, levodopa and methyldopa, their salts and pharmacologically active esters.

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In advantageous embodiments, dosage forms may be formulated in order to obtain a timed pulse release independent of the pH. The preferred manner to achieve such a release, in the case of a basic drug is to add a pharmaceutically acceptable organic acid into the dosage form, according to methods known from one skilled in the art. Such dosage forms are preferred.

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These pharmaceutically acceptable organic acids can be chosen for example among maleic, tartaric, malic, fumaric, lactic, citric, adipic or succinic acid and their acid salts where these exist, in the form of racemates or isomers, where these exist. According to the invention, acids particularly preferred are tartaric, fumaric, citric, and succinic and their acid salts.

The amount of cationic or zwitterionic surfactant which may be used with the present invention may vary but preferably is between 10 and 50% with respect to the amount of ammonio methacrylate copolymer in the coating.

The dosage forms according to the present invention include capsules, tablets, multicoated tablets, granulates.

Various formulations, not limiting the scope of the present invention, illustrating the first object of the invention, that is pharmaceutical dosage forms producing one unique timed pulse, are described hereafter:

(1) Delayed release particles containing a drug:

These are particles of dimension for example 0.2 to 2 mm diameter, comprising in addition to the drug at least a cationic surfactant in the core and with a polymer coating comprising at least one or more ammonio methacrylate copolymers.

The particles may be manufactured by any of the methods well known to one skilled in the art: granulation in a high speed granulator, extrusion followed by spheronisation, gradual coating of a sphere with a mixture comprising the drug etc. The sphere may consist of any commonly used pharmaceutical substance, sucrose, sucrose and starch, mannitol, microcrystalline cellulose.

The particles are coated for delayed release with a coating comprising one or more ammonio methacrylate copolymers. In addition the coating may comprise one or more other polymers impermeable to water and to drug molecules, such as ethylcellulose, cellulose acetate, cellulose acetate butyrate, polyvinyl chloride, polyvinylacetate. The coating may also comprise one or more polymers which are permeable to water, such as hydroxypropylmethylcellulose, hydroxyethylcellulose.

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The composition of the mixture and the amount of coating applied is adjusted to allow gradual hydration of the film and a delayed release profile.

The core may comprise other substances necessary, in particular an organic acid to maintain the pH at the interior of the particle constant. In an advantageous embodiment of the invention the core is separated from the outer coating by a layer water soluble polymers such as hydroxypropylmethylcellulose, hydroxyethylcellulose, and polyvinylpyrrolidone.

The particles may be filled in a unique dosage form as a gelatin capsule.

(2) Delayed release tablets comprising a drug and at least a cationic surfactant in the core and with a polymer coating comprising at least one or more ammonio methacrylate copolymers.

These are formulated by the methods well known to one skilled in the art.

In addition to the drug and the cationic surfactant they can comprise inert pharmaceutical excipients, including one or more diluants, for example microcrystalline cellulose, lactose, mannitol, starch; and may contain other excipients.

These include can one or тоге binders. for example hydroxypropylmethylcellulose, ethylcellulose and povidone, lubricants, for example magnesium stearate, glyceryl stearate, and glyceryl behenate, disintegrants, for example crospovidone, sodium starch glycolate and croscarmellose, glidants, for example talc and colloidal silicon dioxide. In particular a pharmaceutically acceptable acid may be added to ensure liberation of the basic active substances independent of the pH of the external medium.

The tablets can be prepared by compression of a simple mixture or a granulate, followed by coating with a polymer solution.

Minitablets which are also emcompassed in the invention are tablets of dimension 3 mm or less. They can be used for achieving dosage forms for timed pulse release. They can be manufactured using the same components as described above.

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The delayed release tablets can be coated with a layer of polymer coating similar to those described for the multiparticulate systems above. However except in the case of the minitablets some modification of the coating may be required because of the difference in surface area of the dosage form.

It is usually necessary to apply a thicker coating on the tablet than on the particles, and thus a higher proportion of water-permeable polymers can be required in the coating composition. The core may also be separated from the outer coating by a layer of water soluble polymers such as hydroxypropylmethylcellulose, hydroxyethylcellulose, and polyvinylpyrrolidone.

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The delayed release tablets or minitablets may be used alone. The minitablets may also been filled into envelopes such as hard gelatine capsules.

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Moreover, as a further object, the invention also encompasses all dosage forms comprising delayed release coated cores according to the invention combined together to give a "stepped" release profile or with other galenic entities. These other galenic entities can for example be immediate or sustained release systems.

As described above, these further dosage forms can also be used for example in chronotherapeutic treatments, to overcome the first pass effect, or to improve the absorption according to a given part of the gastrointestinal tract.

The other galenic entities may contain the same active substance as the delayed release entity or a different active substance. Indeed, when comprising two different active substance, dosage forms can for example be formulated in order to obtain the complementary treatment described hereinabove.

In particular an object of the present invention is related to pharmaceutical compositions for timed dual release, whereby a first release pulse occurs immediately and a second release pulse is delayed to a fixed time.

Examples of the different types of profiles which may be obtained by combining formulations according to the invention with other galenic entities are shown in figure 1.

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The following formulations illustrate this further object of the invention, that is dosage forms comprising delayed release coated cores according to the invention combined together to give a "stepped" release profile or with other galenic entities:

(1) Capsule comprising the delayed release particles or minitablets according to the invention and an immediate and/or sustained release entities

The required amount of delayed release particles or minitablets according to the invention are combined with one or both of the following

- (i) immediate release (uncoated) particles or minitablets or an immediate release granulate or powder
 - (ii) sustained release particles or minitablets (coated, slow release)

in hard gelatine capsules of the required size.

Particles or minitablets with different delayed release profiles may also be combined to give a "stepped" release profile.

(2) A tablet comprising delayed release particles according to the invention imbedded in a rapidly disintegrating matrix.

The matrix may also comprise the drug substance. Sustained (slow) release particles may be included in addition to the delayed release particles.

Alternatively the tablet may consist of a mixture of delayed release particles and of immediate release non-coated particles comprising the active substance, imbedded in a matrix free from the drug.

Alternatively the delayed release particles may be furthermore coated with a layer comprising the drug and other excipients allowing immediate release from that layer, imbedded in a matrix free from the drug.

Alternatively the delayed release tablet may consist of one or more layers comprising delayed release particles comprising the drug, imbedded in a matrix free from the drug and one or more layers comprising the drug in an immediate release matrix.

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The matrix surrounding the particles should preferably be formulated so that the compression into tablets does not interfere with the integrity of the membrane surrounding the pellets. On contact with fluid the tablet disintegrates, releasing the drug rapidly, from the matrix, or the immediate release pellets, or from the immediate release particle coating, or from the immediate release layer, and then, after a fixed interval of time, releases the drug from the delayed release particles.

In the case of a basic drug the particle may be formulated with a pharmaceutically acceptable organic acid so as to maintain the micro-pH of the particle during release in the neutral pH conditions.

The matrix can consist of inert pharmaceutical substances such as well known to one skilled in the art of pharmaceutical formulation. In particular the matrix can include one or more diluants such as microcrystalline cellulose, lactose, mannitol, starch and one or more disintegrants, for example crospovidone, sodium starch glycolate and croscarmellose. Other excipients may also be included, lubricants, for example magnesium stearate, glyceryl stearate, and glyceryl behenate, binders, for example hydroxypropylmethylcellulose, ethylcellulose and povidone, glidants, for example talc and colloidal silicon dioxide.

(3) Capsule comprising one or more immediate release tablets and one or more delayed release tablets.

The delayed release tablets are prepared as described above. Immediate release tablets can be made exactly the same way, except they are uncoated, do not require a cationic surfactant and do not normally require addition of an acid. Instead of or as well as the immediate release tablet, one or more sustained (slow) release tablets may be included in the formulation.

(4) Multicoated tablets

Delayed release tablets are prepared as described above and press coated with an immediate release soluble or disintegrable coating.

List of figures:

Figure 1 shows examples *in vitro* release profiles, where the full curve shows a delayed release profile (TR), the dashed curve shows the combination of an immediate release with a delayed release profile (IR + TR), and the dotted curve shows the combination of both immediate release and sustained release profiles with a delayed release profile (IR + SR + TR).

Figure 2 shows an *in vitro* dissolution profile of the coated pellets containing alfuzosin hydrochloride of example 1.

Figure 3 shows an *in vitro* dissolution profile of the coated pellets containing alfuzosin hydrochloride of comparative example 1.

Figure 4 shows an *in vitro* dissolution profile of the coated pellets containing alfuzosin hydrochloride of example 2.

Figure 5 shows an *in vitro* dissolution profile of the coated pellets containing alfuzosin hydrochloride of example 3.

Figure 6 shows an *in vitro* dissolution profile of the coated pellets containing alfuzosin hydrochloride of comparative example 3.

The examples which follow illustrate the invention without limiting it:

Example 1: Capsules containing alfuzosine hydrochloride and cetylpyridinium chloride - slow release after a long interval

3325 g of non-pareil beads 16/18 mesh were loaded with alfuzosin hydrochloride by coating in a GPCG3 fluid bed coater-dryer with a suspension of the following condition

alfuzosin hydrochloride	5.0 %	87.5 g
Polyvinyl alcohol ¹	5.0 %	87.5 g
purified water	90.0 %	1575 g

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1100 g of these alfuzosin-coated beads were then coated in a GPCG1 fluid bed coater-dryer using a suspension of the following composition:

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cetylpyridinium chloride	4.3 %	43.4 g
succinic acid	4.7 %	46.9 g
hydroxypropylmethylcellulose ²	5.9 %	59.0 g
purified water	42.5 %	425.0 g
isopropanol	42.5 %	425.0 g

²Pharmacoat 603[®] commercialised by Shin-Etsu

Finally 1000 g of beads above described were coated using a polymer solution of the following composition:

ammonio	methacrylate	5.1 %	119.0 g
copolymer Type B ³			
ammonio	methacrylate	0.3 %	7.0 g
copolymer Type A 4			
acetylated mond	oglycerides ⁵	0.6 %	14.0 g
isopropanol		56.4 %	1316.0 g
acetone		37.6 %	877.3 g

³ Eudragit[®] RS100 commercialised by Röhm Pharma

The dissolution of the beads was measured using the method described in the European pharmacopoeia with the rotating paddle apparatus, at a stirring speed of 100 rpm. Dissolution medium was 500 mL, 0.01M hydrochloric acid at $37^{\circ}\text{C} \pm 0.5^{\circ}\text{C}$. The amount of alfuzosine dissolved was measured by UV spectrophotometry at 330 nm. The dissolution curve obtained is shown in figure 2.

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⁴ Eudragit® RL100 commercialised by Röhm Pharma

⁵ Eastman 9-45 commercialised by Eastman

<u>Comparative example 1</u>: Capsules containing alfuzosine hydrochloride (without cetylpyridinium chloride)

1100 g of the alfuzosin-coated beads, prepared as described in example 1 were coated using a suspension of the following composition:

succinic acid	7.0 %	46.2 g
hydroxypropylmethylcellulose ¹	8.8 %	58.3 g
purified water	42.1 %	277.9 g
isopropanol	42.1 %	277.9 g

¹ Pharmacoat 603[®] commercialised by Shin-Etsu

Finally 1000 g of beads above described were coated using a polymer solution as described in example 1

The dissolution profil of the pellets was determined. The dissolution method was that described in example 1. The dissolution curve obtained is shown in figure 3.

Example 2: Coated pellets

Delayed release pellets containing alfuzosin hydrochloride, tartaric acid and cetylpyridinium chloride as cationic surfactant

1000 g of nonpareil beads 16/18 mesh were coated using a suspension with the following composition:

tartaric acid	6.0 %	78.0 g
hydroxypropylmethylcellulose 1	4.0 %	53.0 g
cetylpyridinium chloride	3.0 %	39.0 g
triethyl citrate	1.4 %	18.2 g
purified water	43.8 %	557 g
isopropanol	43.8 %	557 g

Pharmacoat 603[®] commercialised by Shin-Etsu

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The pellets were then loaded with alfuzosin hydrochloride by coating with the following solution, in a GPCG1 fluid bed coater-dryer:

alfuzosin hydrochloride	8.3 %	78 g
povidone K30 ²	8.3 %	78 g
ethanol	83.4 %	784 g

² Kollidon[®] commercialized by BASF

Finally 1000 g of the pellets were coated using a polymer solution of the following composition :

ammonio	methacrylate	11.40 %	83.4 g
copolymer Type B ³			3 g
ammonio	methacrylate	0.93 %	6.8 g
copolymer Type A 4			_
triethyl citrate		1.37 %	10.0 g
isopropanol		51.80 %	379.0 g
acetone		34.50 %	252.0 g

³ Eudragit[®] RS100 commercialised by Röhm Pharma

The dissolution profile of the pellets in 0.01 M hydrochloric acid was measured using the method described in example 1. The dissolution curve obtained is shown in figure 4.

Example 3: Coated pellets:

Delayed release pellets containing alfuzosin hydrochloride, succinic acid and cocamidopropylbetain as a zwitterionic surfactant

1000 g of nonpareil beads 16/18 mesh were coated using a suspension with the following composition,

⁴ Eudragit[®] RL100 commercialised by Röhm Pharma

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succinic acid	5.63 %	78.0 g
hydroxypropylmethylcellulose 1	3.82 %	53.0 g
cocamidopropylbetain ²	2.81 %	39.0 g
purified water	43.87 %	608 g
isopropanol	43.87 %	608 g

¹ Pharmacoat 603[®] commercialised by Shin-Etsu

The pellets were then loaded with alfuzosin hydrochloride as described in example 2

Finally 1000 g of the pellets were coated using a polymer solution of the following composition:

ammonio	methacrylate	11.40 %	208.5 g
copolymer Type B ³			_
ammonio	methacrylate	0.93 %	17 g
copolymer Type A 4			_
triethyl citrate		1.37 %	25 g
isopropanol		51.80 %	947.5 g
acetone		34.50 %	630 g

³ Eudragit[®] RS100 commercialised by Röhm Pharma

After drying in a ventilated oven, at 30°C for 24 h the dissolution profile of the pellets in 0.01 M hydrochloric acid was measured using the method described in example 1. It is shown in figure 5.

Comparative example 3: coated pellets without surfactant

20 1000 g of non-pareil beads 16/18 mesh were coated using a suspension with the following composition

² Amonyl[®] 380LC commercialised by Seppic

⁴ Eudragit® RL100 commercialised by Röhm Pharma

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succinic acid	5.99 %	78.0 g
hydroxypropylmethylcellulose 1	4.07 %	53.0 g
purified water	44.97 %	585.5 g
isopropanol	44.97 %	585.5 g

¹ Pharmacoat 603[®] commercialised by Shin-Etsu

The beads were then loaded with alfuzosin hydrochloride according to example 1 and finally coated with polymer using the same methods and composition as described in example 3. The dissolution profiles of the pellets were measured as described in example 1. They are shown in figure 6.

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ART 34 AMDT

Claims

- 1. A delayed release coated core producing a timed pulse release, comprising an active substance in its core and a polymer coating comprising at least one or more ammonio methacrylate copolymers, characterised in that the core comprises at least one ore more surfactants, one of said surfactants being a means that diffuses into the polymer coating and at a given level provokes a sudden change in the coating's properties.
- 2. A delayed release coated core according to claim 1, characterised in that 10 the surfactants are cationic or zwitterionic in nature.
 - 3. A delayed release coated core according to claim 1 or 2, characterised in that the ammonio methacrylate copolymers are of type A or B.
 - 4. A delayed release coated core according to anyone of claim 1 to 3, characterised in that the cationic surfactants are chosen among trimethyldimyristoyl-ammonium propionate. dimethyl-dioctadecyl-ammonium bromide, trimethyl-cetyl-ammonium bromide, dimethyl-didodecyl-ammonium bromide. benzalkonium chloride, cetylpyridinium chloride and cetrimide.
 - 5. A delayed release coated core according to anyone of claim 1 to 3, characterised in that the zwitterionic surfactants are chosen among N-alkylbetaines, C-alkylbetaines, N-alkylamidobetaines, N-alkylglycines, phosphatidylcholines and lecithins.
 - 6. A delayed release coated core according to claim 5, characterised in that the zwitterionic surfactant is cocamidopropylbetain.
- 7. A delayed release coated core according to anyone of claim 1 to 6, 30 characterised in that the active substance-is-chosen among diltazem, theophylline, felodipine, verapamil, cionidine, acebutolol, alprenolol, betaxolol, metoprolol, nadolol, propranolol, timolol, captopril, enalapril, fosinopril, tiapamil, gallopamil, amlodipine, nitrendipine, nisoldipine, nicardipine, felodipine, molsidamine, indomethacin, sulindac, indoprofen, ketoprofen, flurbiprofen, fenbufen, fluprofen,

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ART 34 AMDT

diclofenac, tiaprofenic acid, naproxen, mizolastin, terbutaline, salbutamol, betamethasone, prednisone, methylprednisone, dexamethasone, prednisolone, sumatriptan, naratriptan, cimetidine, ranitidine, famotidine, nizatidine, omeprozole, morphine, fenoprofen, ibuprofen, ketoprofen, alclofenac, mefenamic, alfuzosin, prazosin, tamsulosin, levodopa and methyldopa, their salts and pharmacologically active esters.

- 8. A delayed release coated core according to anyone of claim 1 to 7, characterised in that it is a particle, pellet, bead, granule or spheroid, of a diameter comprised between 0.3 and 3 mm.
- 9. A delayed release coated core according to anyone of claim 1 to 7. characterised in that it is a tablet.
- 10. A delayed release coated core according to anyone of claim 1 to 7, characterised in that it is a minitablet.
- 11. A delayed release coated core according to anyone of claim 1 to 10, characterised in that the core is separated from the polymer coating by a layer of water soluble polymer.
- 12. A delayed release coated core according to claim 11, characterised in that said soluble polymer is chosen among hydroxypropylmethylcellulose, hydroxyethylcellulose and polyvinylpyrolidone.
- 13. A pharmaceutical dosage form comprising at least a delayed release coated core according to anyone of claims 1 to 12.
- 14. A pharmaceutical dosage form according to claim 13, characterised in that it takes the form of a tablet, a multilayer tablet, a multicoated tablet or a capsule. 30
 - 15. A pharmaceutical dosage form according to claim 13 or 14, characterised in that coated cores of differing delayed release times are combined together to give "stepped" release profile.

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- 16. A pharmaceutical dosage form according to claim 13 or 14, characterised in that the release coated core(s) is/are combined with other galenic entitie(s), which release is immediate or sustained.
- 17. A pharmaceutical dosage form according to claim 16, characterised in that the other galenic entitie(s) contain(s) a different active substance as in the release coated core(s).
- 18. A pharmaceutical dosage form according to claim 16, characterised in that a first release pulse occurs immediately and a second release pulse is delayed to a fixed time.
 - 19. A capsule according to claim 16, characterised in that it comprises the delayed release coated cores according to claim 8 or 10 and an immediate and/or sustained release entity chosen alternatively among
 - (i) immediate release particles or minitablets or an immediate release granulate or powder,
 - (ii) controlled release particles or minitablets:
 - 20. A tablet according to claim 16, characterised in that it comprises the delayed release coated cores according to claim 8 imbedded in a rapidly desintegrating matrix and alternatively in that
 - (i) the matrix is free of the active substance,
 - (ii) the matrix also comprises the active substance,
 - (iii) sustained release particles are mixed to the delayed release particles,
 - (iv) immediate release particles are mixed with the delayed release coated particles,
 - (v) the delayed release particles are further coated with a layer comprising the active substance, allowing an immediate release,
- (vi) the tablet consists of one or more layers comprising the delayed release particles in the rapidly desintegreting matrix and of one or more layers comprising the active substance in an immediate release matrix.

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- 21. Capsule according to claim 16, characterised in that it comprises one or more immediate release tablets and one or more delayed release tablets according to claim 9.
- 22. Multicoated tablets according to claim 16, characterised in that the tablet is coated with an immediate release soluble or disintegrable coating.

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FIG. 1

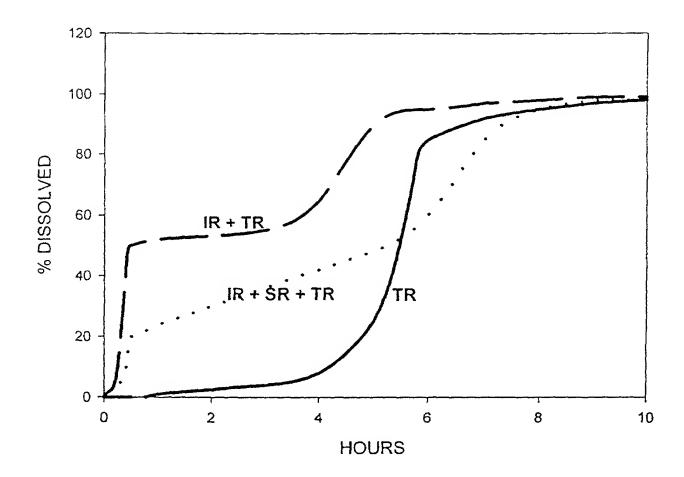
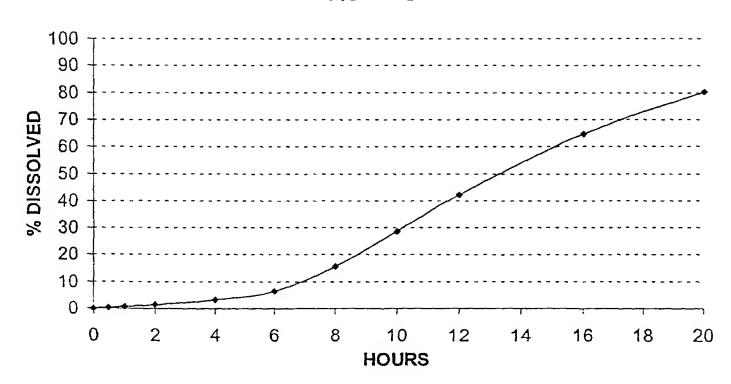


FIG. 2



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FIG. 3

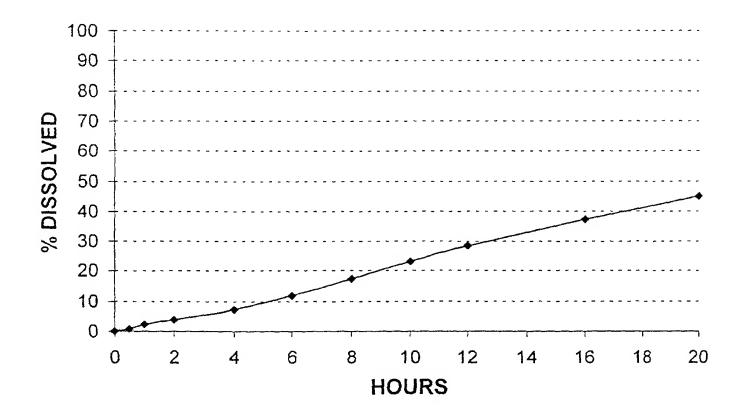
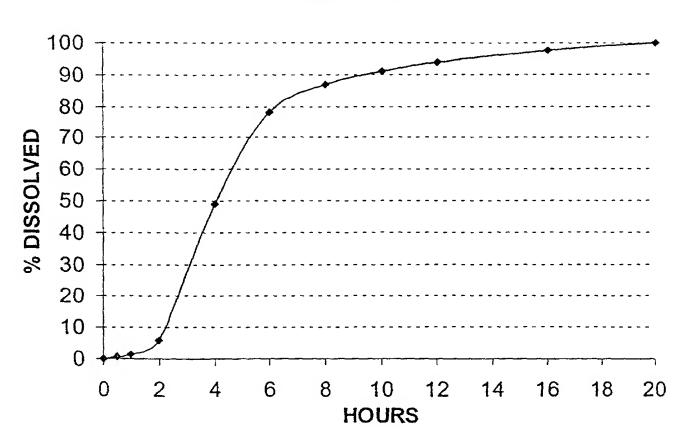


FIG. 4



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FIG. 5

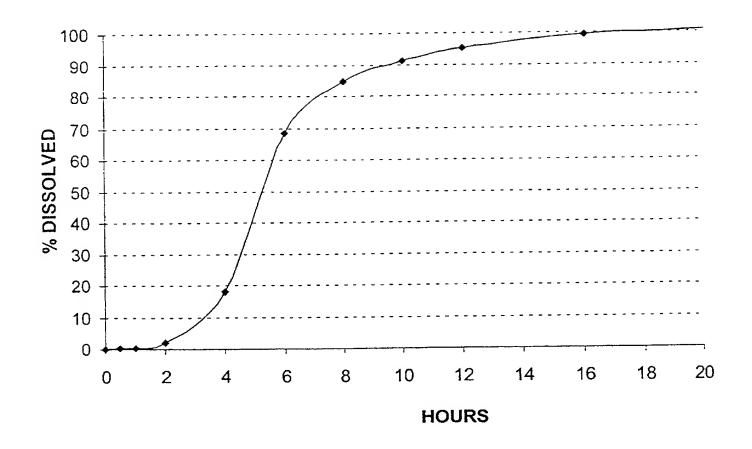
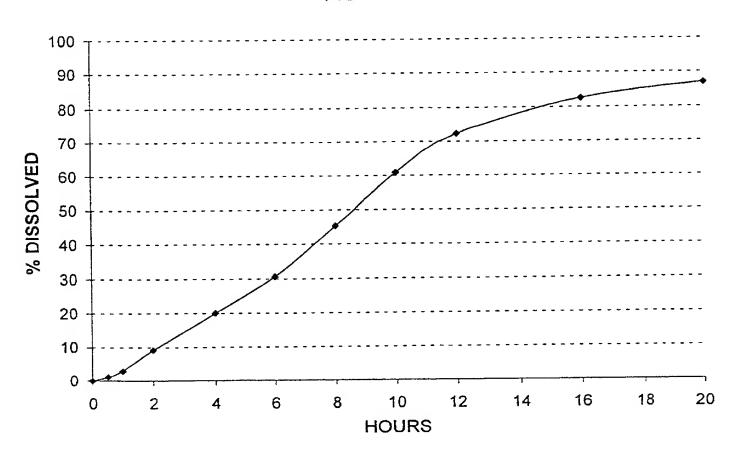


FIG. 6



DECLARATION AND POWER OF ATTORNEY FOR UNITED STATES PATENT APPLICATION

X Original	Suppleme	ental Su	bstitute
As a below-named inven	tor, I hereby declare the	hat:	
My residence, citizenship	p and mailing address	are given below under	my name.
I/We believe that I/we a claimed and for which a patent i			subject matter which is
PHARMACEUTICAL DOSAG LEAST A TIMED PULSE the application for which	GE FORMS FOR C	ONTROLLED RELEA	ASE PRODUCING AT
is attached hereto.			
was filed on Application Serial No.		as United State	es .
and was amended on		(if applicable)	
was filed on	27 June 2000	as PCT Interna	tional
Application No. and was amended on	PCT/EP00/06795	(if applicable)	
I/We acknowledge the conformation known to me/us to the Code of Federal Regulation which became available between international filing date of the collinear to the Code of Federal Regulation which became available between the code of	amendment specificall duty to disclose to the be material to patent s, including for continuen the filing date of continuation-in-part apon priority benefit under	y referred to above. United States Patent a cability as defined in Securation-in-part application the prior application application. der Section 119 (a) - (d)	ons, material information and the national or PCT of Title 35 of the United
States Code of any foreign international application(s) des below and also identify below PCT international application(s me on the same subject matter priority is claimed:	signating at least one any foreign application at least (s)	country other than the ion(s) for patent or involve one country other than	United States identified entor's certificate or any the United States filed by
Country	Number	Filing Date	Priority Claimed Yes No
EUROPE	99 401606.1 —	28 June 1999	$\frac{100}{X}$

	App	lication No.	Filing 1	Date			
	I/We hereby claim benefit under Section 120 of Title 35 of the United States Code of any United States application(s) or PCT international application(s) designating the United States identified below:						
	Application Serial No.	Filing D	eate	Status			
	I/We hereby appoint Michael D. Alexander, Reg. No. 36,080; and Paul E. Dupont, Reg. No. 27,438, or any of them my/our attorneys or agents with full power of substitution and revocation to prosecute this application and to transact all business in the United States Patent and Trademark Office connected therewith. SEND CORRESPONDENCE TO: DIRECT TELEPHONE CALLS TO:						
		102 101	Paul E. Du				
<u> </u>	Patent Department Sanofi-Synthelabo Inc. 9 Great Valley Parkway P.O. Box 3026 Malvern, PA 19355		Telephone No.	(610) 889-6338			
	I/We hereby declare that all statements made herein and in the above-identified application of my/our own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.						
1-60	Full name of first joint inventor Inventor's signature	_AND	RE Frédéric	Date Ly/Nov/Ust			
	Mailing Address/Residence	14 bis rue du Cl	os de Massy, FR-921				
	Citizenship	French /					
2-OT	Full name of second joint inver Inventor's signature	tor <u>LEW</u>	S Gareth	Date 11/15/01			
	Mailing Address/Residence	39 avenue de Pa	ris, FR-91410 <u>DOU</u> I				
	Citizenship	British					

2-07	Full name of third joint inventor	MIGNONNEAU Jerome_			
	Inventor's signature	· · · · · · · · · · · · · · · · · · ·	Date	-16/M/2E	201
	Mailing Address/Residence	1 rue de Jeanne de Laval, FR-49350 SAINT-CLÉMEN	IT-DES-	LEVÉES	FR
	Citizenship	French			
4-00	Full name of fourth joint invento	r RIBARDIERE Agnès			
,	Inventor's signature	Thibai 5	Date	16/1	wol
	Mailing Address/Residence	8 rue de Louvain, FR-92400 COURBEVOIE		·	
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